Effect of Physical Contact (Hand-Holding) on Heart Rate Variability

T. Pishbin, S.M.P. Firoozabadi, N. Jafarnia Dabanloo, F. Mohammadi and S. Koozehgari

Abstract—Heart’s electric field can be measured anywhere on the surface of the body (ECG). When individuals touch, one person’s ECG signal can be registered in other person’s EEG and elsewhere on his body. Now, the aim of this study was to test the hypothesis that physical contact (hand-holding) of two persons changes their heart rate variability. Subjects were sixteen healthy female (age: 20-26) which divided into eight sets. In each sets, we had two friends that they passed intimacy test of J. sternberg. ECG of two subjects (each set) acquired for 5 minutes before hand-holding (as control group) and 5 minutes during they held their hands (as experimental group). Then heart rate variability signals were extracted from subjects’ ECG and analyzed in linear feature space (time and frequency domain) and nonlinear feature space. Considering the results, we conclude that physical contact (hand-holding of two friends) increases parasympathetic activity, as indicate by increase SD1, SD1/SD2, HF and MF power (p<0.05) and decreases sympathetic activity, as indicate by decrease LF power (p<0.01) and LF/HF ratio (p<0.05).

Keywords—Autonomic nervous system (ANS), Hand-holding, Heart rate variability (HRV), Power spectral density analysis.

I. INTRODUCTION

As an electric source, heart sends electrical currents to all parts of the body. The heart generates the largest electromagnetic field in our body. The electrical field that measured in an electrocardiogram (ECG) is about 60 times greater in amplitude than electroencephalogram (EEG) [1]-[2]. As a consistent generator of rhythmic information patterns in our body, and possessing an extensive communication system (nervous system), biochemical communication (hormones) and Energetic communication (electromagnetic fields) [4]. The heart also sends signal to the heart with two branches of autonomic nervous system (ANS).

Figure 1 illustrates how the sympathetic and parasympathetic branches of the ANS influence the sinus node of the heart, thereby modulating heart rate [5].

This figure is not describes all of the functions of the autonomic nervous system of a human, but rather provides an exemplar of those signals and functions which are currently believed to be directly related to the operation of the heart. As illustrated in FIG. 1, the brainstem I receives various input signals, consisting of control and status information, from throughout the body. The brainstem, as the control center of the central nervous system (CNS), continuously summarizes (Σ) all of afferent information and synthesizes appropriate outputs to the heart I via either the sympathetic or parasympathetic subsystems [6].

The output control signals of the sympathetic system, is responsible for increased heart rate in some situation, e.g. in response to feel danger, tend to be relatively low frequency (LF) rhythms. In contrast, the parasympathetic system, which works to limit or repress the effects of the sympathetic system, tend to be relatively high frequency (HF) signals. In general, the parasympathetic system tends to produce a relaxed state whereas the sympathetic a more active, excited state. The
branstorm 1 also receives afferent information from the baroreceptor network, and other receptor neurons, located throughout the heart and in the aortic arch of the heart 2, which are sensitive to stretch (pressure) and chemical changes within the heart 2. As the heart 2 beats, and its walls swell, various baroreceptors are triggered, providing signals as a function of the heart beat, where increased heart rate is generally reflected by increased baroreceptor signals. In response to the sympathetic and parasympathetic control signals from the brainstem 1, the heart rate 2 varies. The sinus node (SN) of the heart 2 is a group of cells which act as a natural pacemaker to initiate the onset of the heart beat at a rate which is non-linearly related to the relative strengths of these autonomic control signals. It has been determined that the heart beats variability, varies according to the shifting relative balance between the parasympathetic and sympathetic signals [6].

Later, neurophysiologists discovered a neural pathway and mechanism whereby input from the heart to the brain could inhibit or facilitate the brain’s electrical activity [7]. Also, they found that during physical contact, one person’s ECG signal can be registered in other person’s EEG and elsewhere on his or her body (Fig. 2) [1].

II. METHODS

A. Subjects

From thirty-eight volunteers (nineteen friends groups) that filled out a health questionnaire and intimacy test of Robert J.sternberg, sixteen female subjects (eight friend groups) had participated in this study. These subjects (age: 20-26) divided into eight sets. In each sets, we had two friends that were healthy and got quorum grade of standard intimacy test. No subject was taking any medication that affect heart rate variability and no subject had diseases such as heart disease, diabetes mellitus or depression and for all subjects signal quality was normal for analysis.

B. Experimental Protocol

To test the hypothesis that when 2 people touch, their heart rate variability properties change because of the exchange of electrical energy produced by their hearts, in this project the experiments were done as followed:

Eight friend sets had participated in this experiment. A total of experiments for each set were conducted on a separate day at the same time (8:30 AM). Each set was seated in comfortable, high-back chair and fitted with ECG electrodes. Prior to each experiment, subjects were asked to turn off their mobile phones and refrain from talking, engaging in exaggerated body movement and from intentionally altering their respiration. The two friends were simultaneously monitored using a 5-minute baseline period during which they seated without any physical contact (control group), followed by a 5-minute hand holding period in which friends remained seated but reached out and held the right hand of her friend (experimental group). We asked friends to hold their right hands because researches had shown that in this hand holding orientation, one person ECG appeared with largest amplitude in the other person EEG [1]. Subjects ECG data had saved as text files for further analysis.

C. Signal Acquisition and Analysis

Disposable silver/silver chloride electrodes were used for
bipolar ECG measurement (limb lead). Electrocardiograph was recorded at 250HZ sampling rate by MP100, BIOPAC System Inc. The signals were stored for latter analysis. R-waves were detected from the ECG signals, based on Pan-Tompkins algorithm [9]. Beat-to-beat RRI (R-to-R-interval) signal was constructed as a series of time difference between the successive heart beats. For spectral analysis purposes, the beat-to-beat data were interpolated and re-sampled at 4 Hz using a cubic spline algorithm. HRV analysis was done with Kubios HRV software [10] and in three categories, i.e. time-domain, frequency-domain and nonlinear methods.

Time domain variables were mean RR, SDNN, RMSSD, NN50 of total HR (%) and HRV triangular index. SDNN is the standard deviation of all RR intervals. RMSSD is the square root of the mean of the sum of the squares of differences between adjacent RR intervals. NN50 count means the number of pairs of adjacent RR intervals differing by more than 50 ms in the entire analysis interval. NN50 of total HR (%) is the NN50 count divided by the total number of all RR intervals. The HRV triangular index means the total number of RR intervals divided by maximum height of the histogram excluding boundaries.

Frequency domain analysis was based on power spectral estimation, which was carried out using FFT based methods by Welch method with FFT length of 1024 points [11].

In this domain, the power was calculated for low frequency (LF, 0.01-0.05 Hz), medium frequency (MF, 0.05-0.15 Hz), and high frequency bands (HF, 0.15-0.5 Hz). The LF region is considered a measure of sympathetic activity. In contrast, the HF region is associated with respiratory sinus arrhythmia and is almost exclusively due to parasympathetic activity. Power in the MF region is thought to be mixed sympathetic and parasympathetic activity. In addition the LF/HF and MF/LF+HF ratio were calculated. LF/HF ratio has been associated with the so-called sympathovagal balance and MF/LF+HF has been highly responsive to changing emotional states [5].

The nonlinear properties of HRV have been analyzed using measures such as poincaré plot [12]-[13], approximate entropy (ApEn) [14]-[15], correlation dimension [16] and detrended fluctuation analysis (DFA) [17]-[18]. ApEn measures the complexity or irregularity of the signal. Large values of ApEn indicate more irregular signal and smaller values of ApEn indicate high regularity [10]. Another method for measuring the complexity or strangeness of the time series is the correlation dimension [10]. The correlation dimension is expected to give information on the minimum number of dynamic variables needed to model the system. DFA also measures the correlation within the signal.

### D. Statistical Analysis

The group values are summarized as mean±SD. Wilcoxon signed rank test was used to compare HRV properties. Statistical analysis was performed using SPSS version 16.0.

<table>
<thead>
<tr>
<th>VARIABLE</th>
<th>CONTROL GROUP</th>
<th>EXPERIMENTAL GROUP</th>
<th>P VALUE</th>
</tr>
</thead>
<tbody>
<tr>
<td>HR Mean (bpm)</td>
<td>76.6±6.16</td>
<td>75.15±6.0</td>
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<tr>
<td>HR std</td>
<td>4.56±1.20</td>
<td>4.55±1.25</td>
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<tr>
<td>RR mean (ms)</td>
<td>791.04±65.02</td>
<td>806.51±62.23</td>
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<tr>
<td>SDNN (ms)</td>
<td>48.24±16.60</td>
<td>49.40±15.15</td>
<td>0.56</td>
</tr>
<tr>
<td>RMSSD (ms)</td>
<td>41.10±18.71</td>
<td>45.60±17.97</td>
<td>0.06</td>
</tr>
<tr>
<td>RR triangular index</td>
<td>11.91±3.60</td>
<td>12.34±2.90</td>
<td>0.71</td>
</tr>
<tr>
<td>pNN50</td>
<td>20.14±19.33</td>
<td>27.65±18.85</td>
<td>0.02*</td>
</tr>
</tbody>
</table>

Values are expressed as mean±SD. * p<0.05.

**RMSSD**: Square root of the mean squared differences between successive RR intervals; **RR triangular index**: The integral of the RR interval histogram divided by the height of the histogram; **pNN50**: NN50 divided by the total number of RR intervals.

### III. RESULTS

#### A. Time-Domain Results

Time domain methods are based on the beat-to-beat or NN intervals. Table I provides time domain data for the 16 subjects. When the group was analyzed as a whole, time domain variables do not demonstrate any differences between two groups (control and experimental groups) except for pNN50 that increased significantly during hand-holding (20.14±19.33 in control group to 27.65±18.85 in experimental group, p<0.05). Also variables showed an increase close to significance in the RMSSD (p=0.06).

#### B. Frequency-Domain Results

In the frequency-domain analysis, a power spectrum density (PSD) estimate is calculated for the RR time series. In this study, the HRV spectrum is calculated with FFT based Welch’s periodogram method. As described by other investigators [21], we divided the power spectrum into three frequency bands: low frequency (LF, 0.01 to 0.05 HZ), medium frequency (MF, 0.05 to 0.15 HZ) and high frequency (HF, 0.15 to 0.5 HZ). The frequency-domain measures extracted from the PSD estimate for each frequency band include absolute total power (ms2) and relative powers of LF, MF, and HF bands, the LF/HF and MF/(LF+HF) power ratios. The band powers in relative units were obtained from the PSD estimate for each frequency band include absolute total power (ms2) and relative powers of LF, MF, and HF bands, the LF/HF and MF/(LF+HF) power ratios. The band powers in relative units were obtained from the absolute values (e.g. relative LF power [%] =absolute LF power [ms2]/absolute total power [ms2] × 100%).

Power spectrum analysis results are summarized in Table II. Frequency domain analysis shows significant decreases in LF/HF ratio (0.95±0.60 in control group to 0.65±0.73 in experimental group, p<0.05) and relative LF power (28.16±11.75 to 17.15±7.61, p<0.01) and significant increases in relative MF power (34.99±15.74 to 41.92±15.03, p<0.05) and relative HF power (36.83±15.38 to 41.42±17.78, p<0.05).
C. Non-linear Results

According to the complex control systems of the heart, it is reasonable to suppose that nonlinear mechanisms are involved in the genesis of HRV [10]. The nonlinear properties of HRV have been analyzed using measures such as Poincaré plot, approximate and sample entropy, detrended fluctuation analysis and correlation dimension (Table III). Comparing non-linear results during hand holding with baseline, HRV parameters such as SD1 (29.16±13.26 to 32.48±13.49, p<0.05) and correlation dimension (2.76±1.33 to 3.33±1.13, p<0.01) increased and a2 decreased significantly (0.83±0.15 to 0.71±0.14, p<0.05).

IV. DISCUSSION & CONCLUSION

The results show that HRV is changed by physical contact (hand-holding). The changes in HRV during hand-holding were detected both by linear and non-linear methods. Among the parameters, the linear variables, pNN50, HF, MF, LF and LF/HF and the non-linear variables SD1, SD1/SD2, a2 and correlation dimension changed significantly in the experimental group compared to the control group. Non-linear variables such as SD2 (ms) and Poincare (SD1/SD2) have been analyzed quantitatively by calculating the standard deviations of the distances of the RRI(i) to the lines y = x and y = -x + 2*RRIm, where RRIm is the mean of all RRI(i).

Table III shows the comparison of non-linear results between the control and experimental groups. The non-linear variables a1 and a2 showed significant changes in the experimental group compared to the control group. Non-linear results during hand-holding show increased parasympathetic activity.

With regard to frequency domain measures, the MF components (0.05-0.15 Hz) in HRV are mediated both sympathetically and parasympathetically and depend on baroreflex. The LF components (0.01-0.05 Hz) are mediated sympathetically and the HF (0.15-0.5 Hz) oscillations of HRV reflect vagal activity only. Our observation suggests that physical contact (hand-holding) caused parasympathetic activation and reduced sympathetic activation, as indicated by increased HF (28.16±11.75 to 17.15±7.61, p<0.01). On the other hand, it has been shown in a number of the studies that positive emotions such as appreciation create increase in parasympathetic activation. Positive emotions change the sympathovagal balance which may be beneficial in the treatment diseases such as hypertension and reduce the likelihood of sudden death in patients with congestive heart failure and coronary artery disease [5]-[6]. The results of work in this area show a significant decrease in the LF/HF ratio and significant increases in LF power (p<0.01), HF power (p<0.01) and in the MF/LF+HF ratio (p<0.01) during positive emotions [5]-[8]. Hence, considering power spectral results and changes in power spectral bands, it seems that subjects (friends) had positive emotions during hand-holding.

Among the non-linear HRV properties, the Poincare plot has been analyzed quantitatively by calculating the standard deviations of the distances of the RRI(i) to the lines y = x and y = -x + 2*RRIm, where RRIm is the mean of all RRI(i). These standard deviations named as SD1 and SD2, respectively. SD1 is related to the fast beat-to-beat variability in the data (used as an indicator of vagal influence), while SD2 describes the longer-term variability of RRI (used as an indicator of sympathetic influence) and the ratio SD1/SD2 describe the relationship between these components [11]. Similar to frequency results, increase of SD1 (29.16±13.26 to 32.48±13.49, p<0.05) and SD1/SD2 (0.83±0.15 to 0.71±0.14, p<0.01) shows increase of parasympathetic activity during hand-holding. Also, compare nonlinear results of control and experimental groups show a significant increase in correlation dimension (2.76±1.33 to 3.33±1.13, p<0.01).

So in this study, we found that physical contact (hand-holding) caused parasympathetic activation, as indicated by increased SD1, SD1/SD2, HF and MF power. These HRV changes that occur during skin-to-skin contact (hand-holding) may because of heart signal transference from one person to another person. As we said, the electrical activity of the heart, cause an electrical current in the body (as a volume conductor).
and by the physical contact of two persons (contact of two volume conductors) this current can flow in the other’s body and vice versa. This signal can change one person’s HRV directly by changes her ECG signal or indirectly by affects her sympathetic and parasympathetic signals. Of course we should note that other factors also can play role in these HRV changes. For example as we said, emotions have principal role on the rhythm of the heart and it should be considered and it is possible that when two friends touch, temperature of their hands, and the other feelings or senses that exchange during a touch, influence these changes and many other factors that we don’t have any information about them.

The experiments in this study represented an initial attempt to identify HRV changes during physical contact. In future experiments, increase of statistical population in different ages and sexes can give us better results. It is our hope that these data will encourage interested researchers to investigate the answers of many unanswered questions that have been raised by this work.

ACKNOWLEDGMENT

This work was done in the Biomedical Engineering Department, Azad University of Science & Research, Tehran, Iran.

REFERENCES


